



## **Fatigue Characterizations Modifying for Below Knee Prosthesis Composite Materials by using Natural Knitted Kenaf Reinforcement Fibers**

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### **Abstract**

This research approach of several composite materials with 12 layers were suggested from perlon, kevlar and woven carbon fibers, and natural knitted kenaf, the purpose findings mechanical, physical properties and fatigue life that help to use the socket with good design at longest period. There are two best types of composite materials are used for to analysis of the fatigue and tensile properties of prosthetic socket below knee which laminated by using vacuum system. The pressure inside the stump of patient and the socket was 165 kpa. Originality of using natural kenaf fibers led to the improvement of the maximum tensile strength 39.35% and safety factor of 2.52, with research limitations at the lowest costs and longest period of time. So, the experimental and numerical techniques were used to calculate the fatigue characterizations for effect of kenaf reinforcement fiber of composite materials used. Therefore, the experimental work included manufacturing for composite samples with different lamination layers and various layer number of kenaf fiber, in addition to, calculated the mechanical properties and fatigue life of its samples. The experimental results of fatigue have a good agreement with those obtained using the Finite Element approach. It was found that sample with kenaf has a maximum number of cycles up to failure =  $18.35 \times 10^5$  cycle at stress ratio ( $R = -1$ ). The analytical part, using ANSYS2020 R2 to model (BK) from suggested materials with and without kenaf for the patient suffering from lower knee amputation for diabetes. Practical implications of experimental and numerical methodology showed that kenaf fibers have achieved the requirements of safety.

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**Keywords:** Below Knee; Prosthetic Socket; fatigue test; Natural Fibers; FEM.

### **1. Introduction**

Below -knee amputations or "BK" amputations, known as transtibial amputations, represent the largest percentage of lower limb amputations [1]. Components of a prosthetic limb are, socket, pylon, ankle, and foot as shown in Figure 1, [2]. The problem of stress and deformities of the socket (amputation below the knee BK), such as sagging and socket fracture caused resulting patient's weight during movement and walking, which causes discomfort to the patient and instability of his movement [3-5]. This will cause a fatigue in the socket due to the induced tension and compression stresses developed during the gait cycle. Therefore, many researchers presenting study for fatigue characterization of composite materials used to manufactured the socket structure as,

Kahtan Al-Khazraji et.al (2012), studied the tensile and fatigue properties of lower prostheses sockets (BK) made of composite materials. They used epoxy with woven fibers (carbon, glass, perlon), with micro and nano silica particles using vacuum technology. Evaluation of fatigue characteristics using (ANSYS-11) program [6]. Saif M. Abbas et.al (2018), examined mechanical properties as a safety factor, fatigue behavior, Von Mises stress in the amputation prosthesis. Using ANSYS 14.5, the safety factor was (2.43) for best group and considered safe and acceptable in designs [7].

Ahmed. K. Abdulameer et.al (2018), investigated theoretically and numerically the fatigue strength of the Syme's prosthetic socket. Suggested materials to find the resistance material to repeated loads during the walking cycle. The model is made of a 6-layer Perlon fiber, 4-layer carbon woven and acrylic resin, allowed safety factor (4.637) [8]. Ehab N. Abbas et.al (2020), studied the fatigue characterization to prostheses materials to maintain the dynamic load that the patient is exposed to during the gait cycle. Sequence was chosen (perlon, glass, carbon, Kevlar). They performed a fatigue test for constant and variable amplitude Low-High and High-Low fatigue test to obtain the correct age for consideration, Finite element technique was used to calculate the fatigue behavior of composite materials [9]. Where the papers submitted showed that the use of reinforced fibers in the manufacture of prostheses are necessary to modify the characteristics of the manufactured socket. Fatigue and fracture are one of the main sources of failure sockets that result in unreliable wear and cause socket failure plus the cost of replacing the prosthesis [10, 11]. The composite material used in socket manufacturing was developed by adding natural fibers such as cotton, flax, kenaf and sisal in order to improve the properties of the composite material and obtain the best properties of the fatigue at the lowest weight and cost.

A.P. Irawan et.al (2011), presented a study on the development of (BK) socket manufacturing by using natural fibers. They chose natural ramie fiber reinforced with epoxy composite (RE) instead of glass fiber (FGP) reinforced with polyester composite [12]. Agustinus P. Irawan et.al (2015), proposed to develop the production of the (BK)Socket prosthesis by adding natural fibers Rattan fiber as reinforcing material with epoxy (RFREC) have good strength and light weight. The socket product an alternative that can be used more comfortably and safely, add to advantages of using natural fibers that can be recycled as environmentally friendly [13]. Bushra.H. Musa (2016), presented on improving the mechanical properties of the composite material of socket reinforced with natural Kenaf fibers [14]. J.K. Odusote et.al (2016), investigated the mechanical properties of pineapple leaf fiber reinforced thermoset composites as possible alternatives to the glass fiber reinforced (AK) prosthetic socket [15]. Jumaa S. Chiad et.al (2017), suggested using of monofilament lamination, perlon fibers and cotton in the manufacture of prosthetic socket (AK). The socket was simulated by using ANSYS. The results show an increase in Young's modulus and a decrease in tensile, yield stress, deformation and increase the stress endurance and the safety factor of 0.323 to 1.05 of the suggested material [16].

The research aims to find composite materials consisting of several layers with natural fibers (kenaf) that are used in the manufacture the below knee (BK) socket with good fatigue life and low cost and high efficiency for the comfort of the patient. So, the experimental and numerical techniques used to calculate the fatigue characterization for materials.



Figure 1. Components of a prosthetic limb [2].

## 2. Fatigue Methodologies

Fatigue is an important phenomenon to be taken into the behavior of mechanical components subjected to constant and variable amplitude loading. Fatigue is the process of a cumulative damage in a benign environment that is caused by repeated cyclic loads. Generally, there are three main techniques used in fatigue analysis which are: stress life, strain life and fracture mechanics. In this work, the stress life approach had been considered to predict the cyclic life of specimens used for the alternating bending machine, [17-20].

### 2.1 Constant-amplitude loading

Constant-amplitude load histories can be represented by a constant load (stress) range, ( $\Delta\sigma$ ); a mean stress  $\sigma_m$ ; an alternating stress or stress amplitude,  $\sigma_a$  and a stress ratio R, Constant stress range,

$$\Delta\sigma = \sigma_{\max} - \sigma_{\min} \quad (1)$$

Mean stress,

$$\sigma_m = \frac{\sigma_{\max} + \sigma_{\min}}{2} \quad (2)$$

Stress amplitude,

$$\sigma_a = \frac{\Delta\sigma}{2} = \frac{\sigma_{\max} - \sigma_{\min}}{2} \quad (3)$$

Stress ratio,

$$R = \frac{\sigma_{\max}}{\sigma_{\min}} \quad (4)$$

$R = -1$  and  $R = 0$  are two common reference test conditions used for obtaining fatigue data. In this work, the type of loading conditions was fully reversed bending loading ( $R = -1$ ) due to availability of fatigue testing machine and at the same time for certain application different R ratios have been employed by using finite element analysis.

### 2.2 Basquin's model

The stress-life curve is a graphical representation of fatigue data. It represents the relationship between fatigue life, in cycles, and the applied stress amplitude. Basquin's relation the most commonly used model and provides an analytical expression of the S-N curve, for finite life (low or high cycle fatigue). By using this technique an estimation of life prediction, with little information on the material can be obtained. The simple Basquin's curve is,

$$\sigma_a = a \cdot N_f^b \quad \text{Basquin Equation} \quad (5)$$

Where  $\sigma_a$  is stress amplitude (MPa) and  $N_f$  is the number of cycles to failure; the parameters a, b are both constant, depending on the material and on the geometry, respectively. The value of fatigue limit is not clearly obvious on the S-N curve; therefore, the fatigue limit can be calculated by using the fatigue life estimation equation at 106 cycles [21]. Fatigue ratio has calculated theoretically according to the equations [22],

$$\text{Fatigue ratio}(R_r) = \frac{\text{Endurance Limit}(\sigma_e)}{\text{ultimat tensile strength}(\sigma_{ts})} \quad (6)$$

### 2.3 Modeling of Prosthetic Socket Using ANSYS

The finite element method (FEM) is now widely used in a variety of fields in engineering and science, [23-34]. In this work, ANSYS-2020R2 software was used. The meshing process has been done by choosing

the volume, and then the shape of element was selected as tetrahedron (Automatic meshing) as shown in Figure 2, [35-50]. This mesh has 20097 nodes and 9750 elements, as shown in Figure (3).

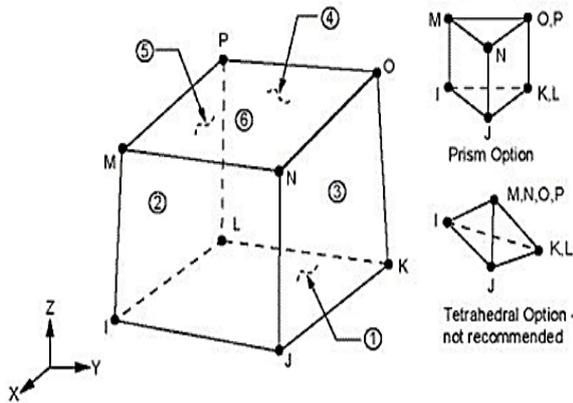


Figure 2. Solid 185 element, [51].

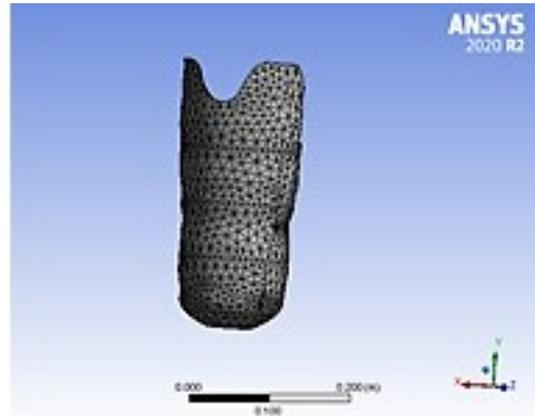


Figure 3. Mesh of the socket Model.

The aim of this analysis is to investigate the stresses and safety factor of socket at maximum pressure the interface pressures between socket and stump was (165 Kpa) for patient 80 kg by applying uniformly distributed on the inner surface of the socket, and from the experimental test f- socket for asimilar case study patient with a right leg amputation (BK) of 85 kg. The analysis was done in the two cases for to best laminations (group G &D\_f). The physical properties (e.g. density) and mechanical properties e.g. ultimate stress ( $\sigma_{ult}$ ), Modulus of elasticity (E) and fatigue life for two cases mentioned above were estimated in the experimental part (tensile test) of this work.

**3. Experimental Procedures**

*3.1 Materials used in below knee socket lamination*

Materials needed in the lamination of the below knee socket for this study are: Natural knitted kenaf, Carbon fiber, Kevlar Fibers, Perlon stockinet and Lamination 617H19 resin. Hardening powder, Polyvinyl alcohol PVA bag and Materials for Japson mold is used with vacuum system to prepare the test samples according to the Table 1.

Table 1. The selected lamination of composite materials for prostheses.

| Group name           | Lamination Lay-up Procedures  | Thickness (mm) |
|----------------------|---|----------------|
| Group G/withot kenaf | (1)perlon+(2)carbon fiber+(1) Kevlar fiber+(4)perlon + (1) Kevlar fiber +(2)carbon fiber +(1)perlon                                     | 3.8            |
| Group D/ with kenaf  | (1)Perlon+(2) Carbon fiber +(1) Kevlar fiber+(1) kenaf fiber +(2) Perlon +(1) kenaf fiber +(1) Kevlar fiber+(2) Carbon fiber+ (1)Perlon | 4              |

*3.2 Tensile Test*

Three specimens of two samples were prepared using a CNC machine based on the recommendation of ASTM D638 [52] as Figure 4, the test was carried out at the speed of 5 mm/sec and at room temperature.

*3.3 Fatigue Test*

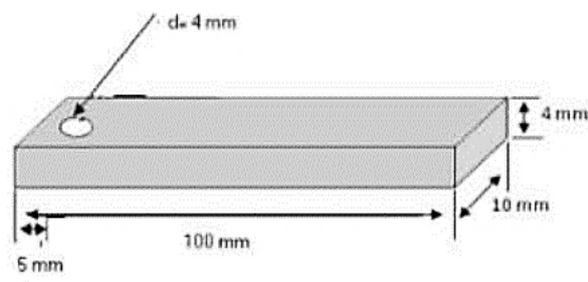
The alternating bending fatigue machine used in this test with speed of motor 1440 rpm, Voltage 230 V, Frequency 20Hz, Power 400W. Ten specimens were prepared for without and with kenaf according to the machine's manual test, where, ten samples required test for each fatigue test samples, [53-60]. Figure 5.a shows the dimensions of specimen and Figure 5.b shows fatigue machine. The specimen was subjected to a perpendicular deflection according to its axis at one side of the specimen and a stress ratio of R= - 1 (tension- compression), while the other side was fixed. The deflection depends on composite material and subjected to a lower speed compared with the metal. A nomogram is used to determine the cantilever length of the specimen and the required deflection to apply the desired stress. A dial gage is used to select the

deflection. The stress was applied to the specimen until a crack appeared. The specimens before and after test are shown in Figure 5.c and d. This test denotes the stress- the number of cycle diagram (S-N) which gives the failure behavior of material stress, to create a curve alternating stress ( $\sigma_a$ ) values are determined form, [61],

$$\sigma_a = \frac{1.5 E_b * t_a * \delta}{l^2} \quad (7)$$



Figure 4. Tensile samples before and after test respectively.



(a) tander dimensions of fatigue specimens



(b) Alternating-bending fatigue testing machine



(c) Fatigue sample before test



(d) Fatigue sample after test

Figure 5. Fatigue specimens and machine.

#### 4. Results and Discussion

After the tensile test was done, the average value for three specimens were calculated. The ultimate stress ( $\sigma_{ult}$ ) for Group G/without kenaf (134.47Mpa) and the modulus of elasticity (16.78Gpa). The ultimate stress ( $\sigma_{ult}$ ) for Group D/with kenaf (187.39Mpa) and the modulus of elasticity (17.49Gpa). These properties were used later to conduct the fatigue test and to be imported to ANSYS 2020 software to simulate the prosthetic socket.

4.1 Fatigue Test Results

The results of fatigue test for best laminations (group G & D\_f) according to maximum ultimate stress. The fatigue S-N curve was drawn by plotting a curve which reflecting the experimental data of fatigue tests by using a power formula of least squares regression [62-68], as shown in Figure (6) which shows stress to number of cycles (S-N) curves for two composite materials. While Table 2 explains the equation of fatigue life for each lamination materials gives the fitting equation of stress and a correlation coefficient (R2) where it is considered important parameter to know how strong the relationship between stress and number of cycles for the proposed laminations where the closer is R2 to 1, the stronger is the relationship between  $\sigma$  and N.

The figure and the table explain that the fatigue life was highly increased in the lamination of kenaf. Compared with other lamination without kenaf. This means that the suggested material has high fatigue properties and a long time without need to replacing or maintenance. The presence reinforcement with kenaf fibers anticipated strong high tensile properties suggest that would be orientated with their longitudinal axis perpendicular to the crack wave, effective in bridging the initial crack and preventing crack propagation, further enhancing the mechanical integrity of the composite material [69-72]. This enhancement has advantages for kenaf lamination materials in manufacturing prostheses can be shown that the modifying for fatigue behavior for composite materials reinforcement with kenaf, and that because of decrease in the rate of crack. Also, the endurance stress of the best lamination with kenaf was increased (38.97%) percentage compared with group G lamination without kenaf and without increasing the weight for composite materials. Hence the fatigue strength of materials is a function of its stiffness. In other words, materials with higher modulus of elasticity and higher maximum tensile strengths possess higher fatigue strength [61]. It is noted that this type of composite material has a high S-N curve because carbon fibers, Kevlar and kenaf are described by high fatigue properties. So, by using this type of material in the manufacturing of socket, the socket could remain for longer time without fracture as compared to polypropylene material.

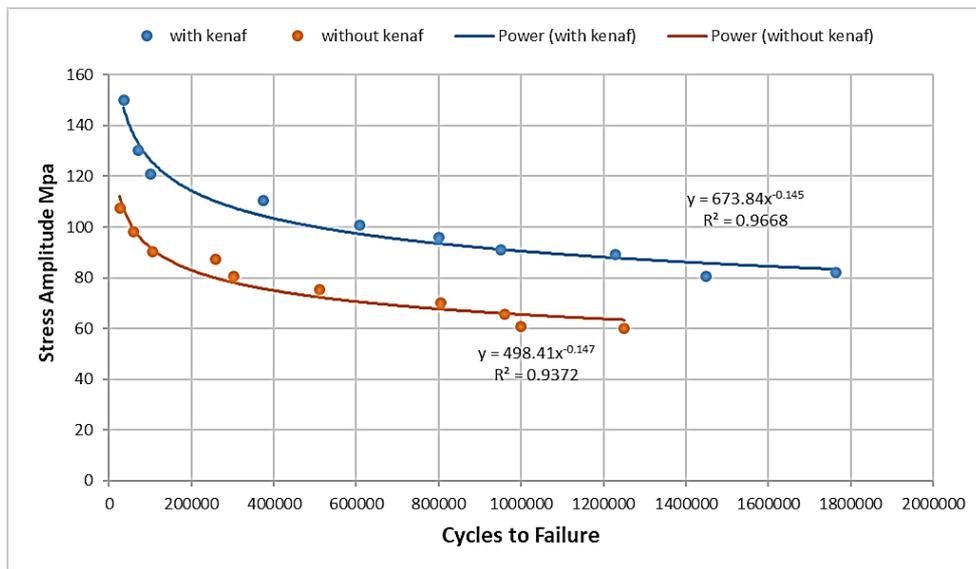


Figure 6. S-N curve for fatigue test.

Table 2. Fatigue life equations for all composite materials.

| Name of lamination    | Fatigue life equation   | Endurance limits Mpa at 10 <sup>6</sup> | Fatigue ratio R <sub>r</sub> | R <sup>2</sup> |
|-----------------------|-------------------------|---|------------------------------|----------------|
| Group G/without kenaf | $Y = 498.41 x^{-0.147}$ | 65.4                                    | 0.485                        | 0.9372         |
| Group D/ with kenaf   | $Y = 673.84 x^{-0.147}$ | 90.89                                   | 0.486                        | 0.9668         |

4.2 Numerical Results

The aim of this analysis is to investigate the equivalent (Von-Mises) stress and safety factor of prosthetic socket. According to the Von-Mises theory that considers the yield stress as fatigue criteria,

( $\sigma_e < \sigma_y$ , safe), ( $\sigma_e = \sigma_y$ , critical) and ( $\sigma_e > \sigma_y$ , failed).

Where, ( $\sigma_e$ ) is the equivalent stress, and ( $\sigma_y$ ) is the yield stress.

The safety factor for fatigue is safe in design if the safety factor about or more than (1.25) [73].

### I. Fatigue Life Results

Fatigue life shows the available life for a given fatigue analysis. Counter plots were used to display the overall distribution of life throughout the socket for each type of composite used in this study the lamination without kenaf (group G) and with kenaf (group D\_f) for analysis at 165 kpa and experimental f-socket as shown in Figures (7), (8) and (9), (10) respectively. In stress life analysis with constant amplitude, if the equivalent alternating stress is lower than the lowest alternating stress defined in the S-N curve, the life at that point will be used [6]. From the results, 165 kpa and for f-socket results, it was noticed that lamination with kenaf has a longer fatigue life than the lamination without kenaf.

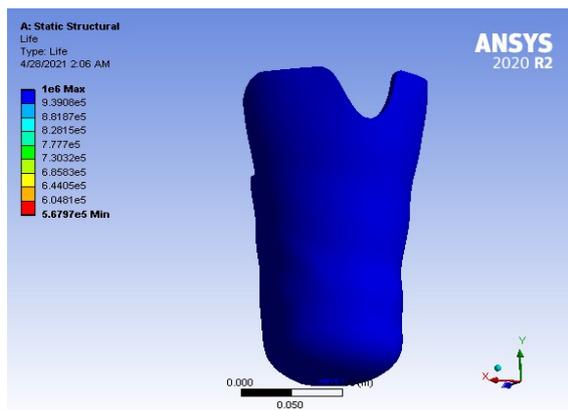


Figure 7. Contours of fatigue life distribution for the lamination without kenaf prosthetic socket, for group G at 165 kpa.

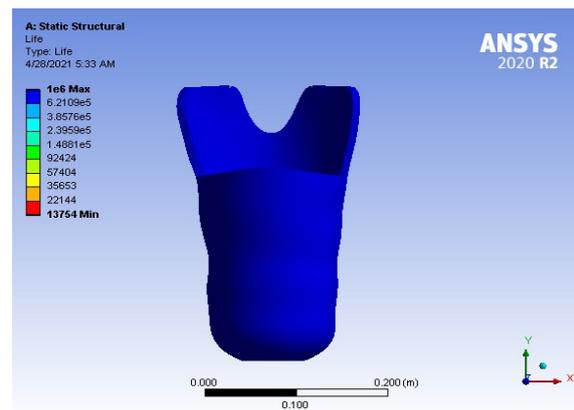


Figure 8. Contours of fatigue life distribution for the lamination with kenaf prosthetic socket, for group D at 165 kpa.

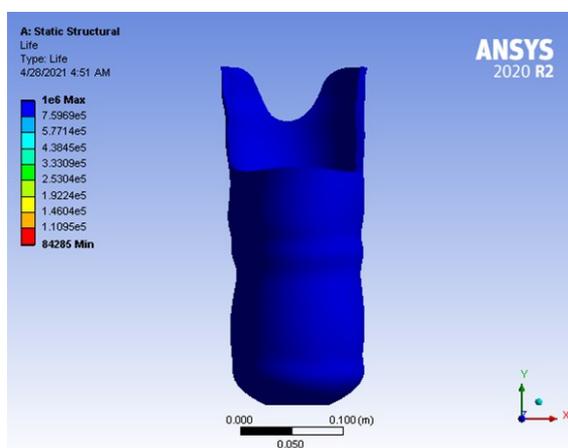


Figure 9. Contours of fatigue life distribution for the lamination without kenaf prosthetic socket, for group G with f-socket.

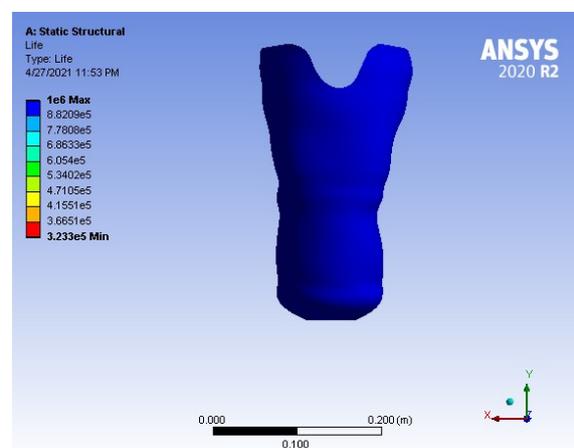


Figure 10. Contours of fatigue life distribution for the lamination with kenaf prosthetic socket, for group D with f-socket.

### II. Fatigue factor of Safety Results

These are counter plots with respect to fatigue failure at a given design life. In Ansys, Maximum factor of safety displayed is 15, values less than one indicates failure before the design life has been reached [74-75]. The safety factor for the suggestion composite material groups of the socket model is passed in design, note that the value of safety factor varies from region to region depending on the distribution of stresses generated and the endurance stress for each group of composite materials. Each color indicates a certain gradient of values for the safety factor. The minimum safety factors are obtained at 165 kpa and f-socket for the lamination without kenaf (group G) and with kenaf (group D\_f) of prosthetic socket respectively.

It can be noticed the distribution of safe and unsafe regions of the composites. At 165 kpa lamination without kenaf prosthetic socket (group G) are 1.43, and 1.58 with kenaf (group D\_f) as shown in Figures (11) and (12) respectively.

At f-socket results lamination without kenaf (group G) the minimum safety factors were 1.75 and 2.52 with kenaf (group D\_f) as shown in Figures (13) and (14) respectively. The fatigue analysis used in the present work is based on fully reversed bending  $R = -1$  (tension– compression) life in case full reversal. In both investigations, 165 kpa and f-socket we note that the minimum safety factors are higher with kenaf lamination improved 10.4% at 165 kpa and 44% for f-socket.

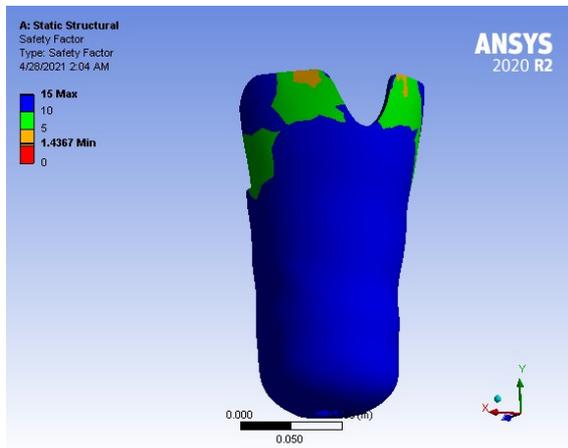


Figure 11. The minimum equivalent safety factor for the lamination without kenaf prosthetic socket (group G) at 165kpa.

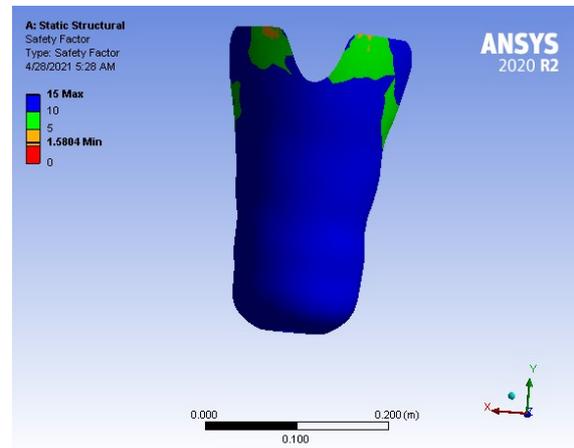


Figure 12. The minimum equivalent safety factor for the lamination with kenaf prosthetic socket (group D\_f) at 165kpa.

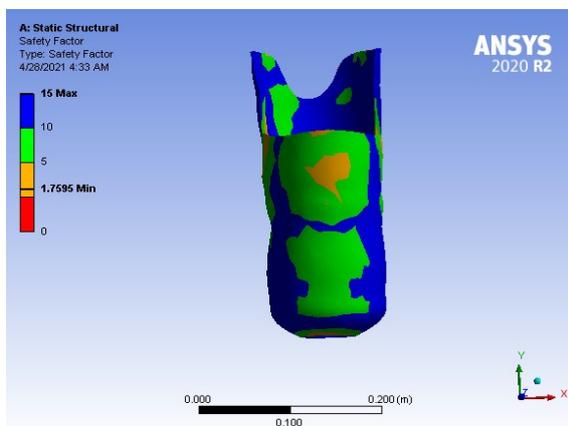


Figure 13. The minimum equivalent safety factor for the lamination without kenaf prosthetic socket (group G) for f-socket.

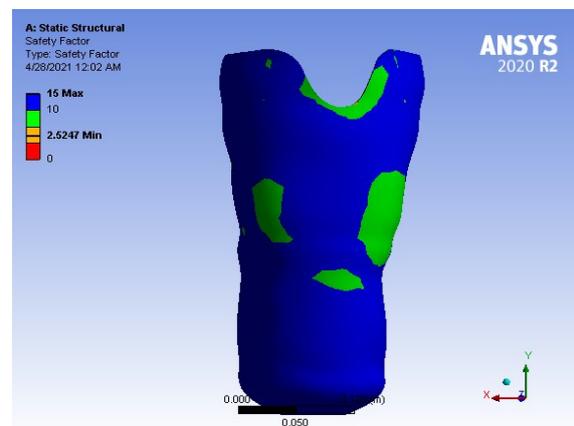
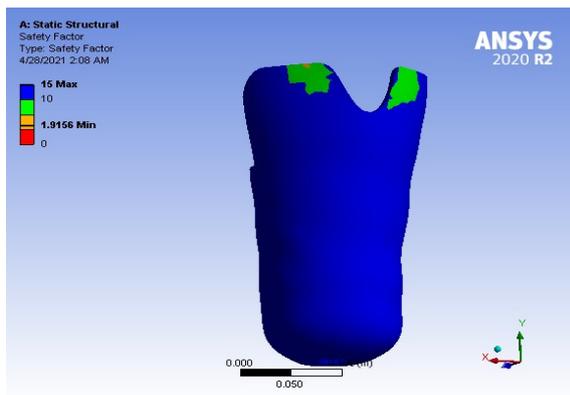


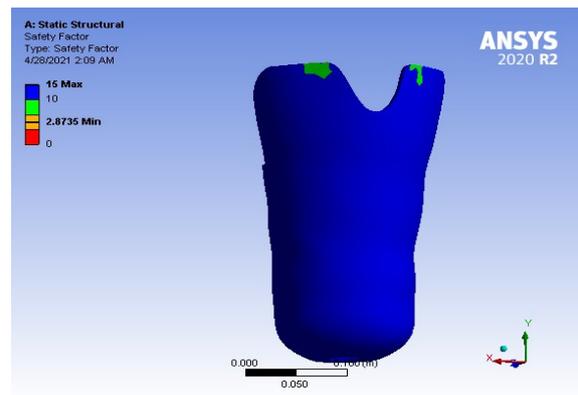
Figure 14. The minimum equivalent safety factor for the lamination with kenaf prosthetic socket (group D\_f) for f-socket.

### III. The effect of the stress ratio on the safety factor

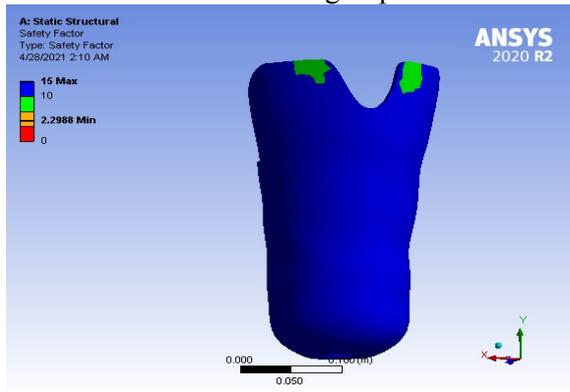
The stress ratios were changed mathematically through FEA Ansys 2020R2 to investigate the extent of its effect on the safety factor for both the analytical and experimental part of the lamination with kenaf (group D\_f) and without kenaf (group G). Safety factor data collected by FEA under constant loading conditions based on various load ratios:  $R = (-1, -0.5, 0, 0.25, 0.5)$  according Good Man Theory [21], these results are found for two laminations. It is found that the maximum fatigue safety factor. Figure 15 and 16 shows the minimum equivalent safety factor for the lamination without kenaf (group G) and for the lamination with kenaf prosthetic socket (group D\_f) respectively, at 165 kpa with different values of stress ratio. And Table 3 explains the results. Figure 17 and 18 show the minimum equivalent safety factor without kenaf (group G) and with kenaf (group D\_f) respectively, for f-socket with different values of stress ratio. Table (4) explains the results.



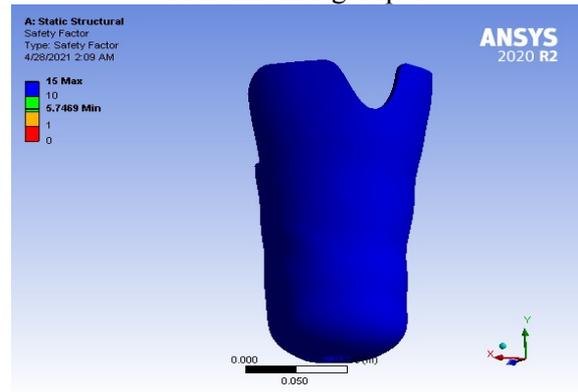
a. stress ratio group B



b. stress ratio group C

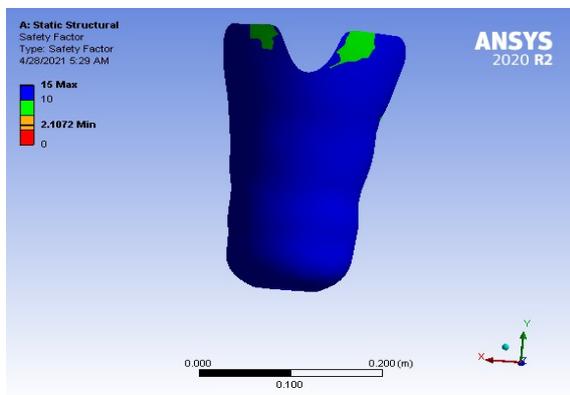


c. stress ratio group D

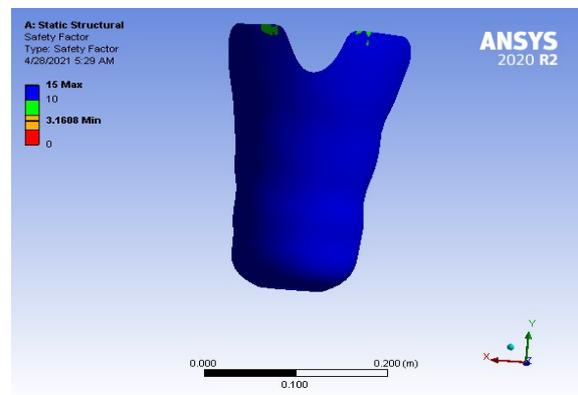


d. stress ratio group E

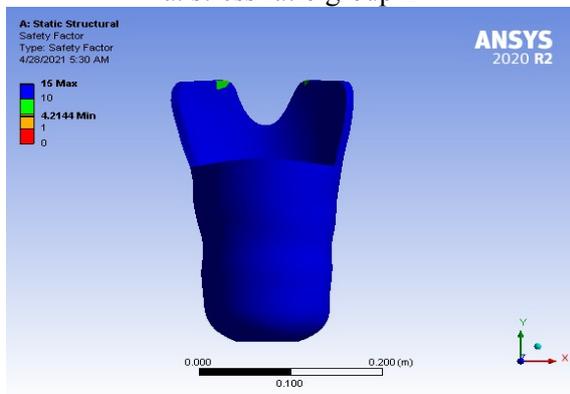
Figure 15. The minimum equivalent safety factor for the lamination without kenaf prosthetic socket (group G) at 165 kpa with different values of stress ratio.



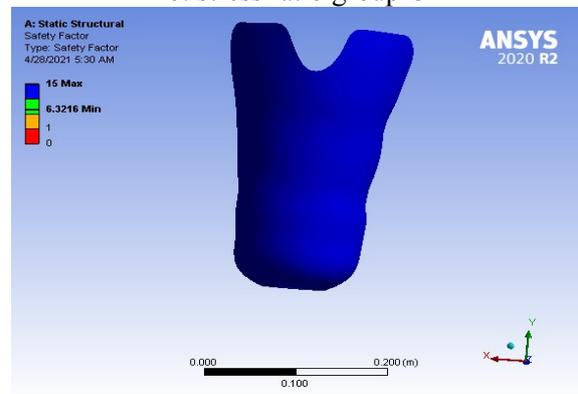
a. stress ratio group B



b. stress ratio group C



c. stress ratio group D



d. stress ratio group E

Figure 16. The minimum equivalent safety factor for the lamination with kenaf prosthetic socket (group D\_f) at 165kpa with different values of stress ratio.

Table 3. The stress ratio values and minimum equivalent safety factor at 165kpa.

| No. | Stress ratio | Safety factor | Group name             |
|-----|--------------|---------------|------------------------|
| A   | -1           | 1.436         | (groupG) without kenaf |
| B   | -0.5         | 1.915         |                        |
| C   | 0            | 2.87          |                        |
| D   | -0.25        | 2.298         |                        |
| E   | 0.5          | 5.476         |                        |
| A   | -1           | 1.508         | (groupD) with kenaf    |
| B   | -0.5         | 2.108         |                        |
| C   | 0            | 3.160         |                        |
| D   | 0.25         | 4.214         |                        |
| E   | 0.5          | 6.321         |                        |

Table 4. The stress ratio values and minimum equivalent safety factor for f-socket.

| No. | stress ratio | safety factor | Group name             |
|-----|--------------|---------------|------------------------|
| A   | -1           | 1.759         | (groupG) without kenaf |
| B   | -0.5         | 2.346         |                        |
| C   | 0            | 3.519         |                        |
| D   | 0.25         | 4.692         |                        |
| E   | 0.5          | 7.038         |                        |
| A   | -1           | 2.524         | (groupD) with kenaf    |
| B   | -0.5         | 3.366         |                        |
| C   | 0            | 5.049         |                        |
| D   | 0.25         | 6.732         |                        |
| E   | 0.5          | 10.099        |                        |

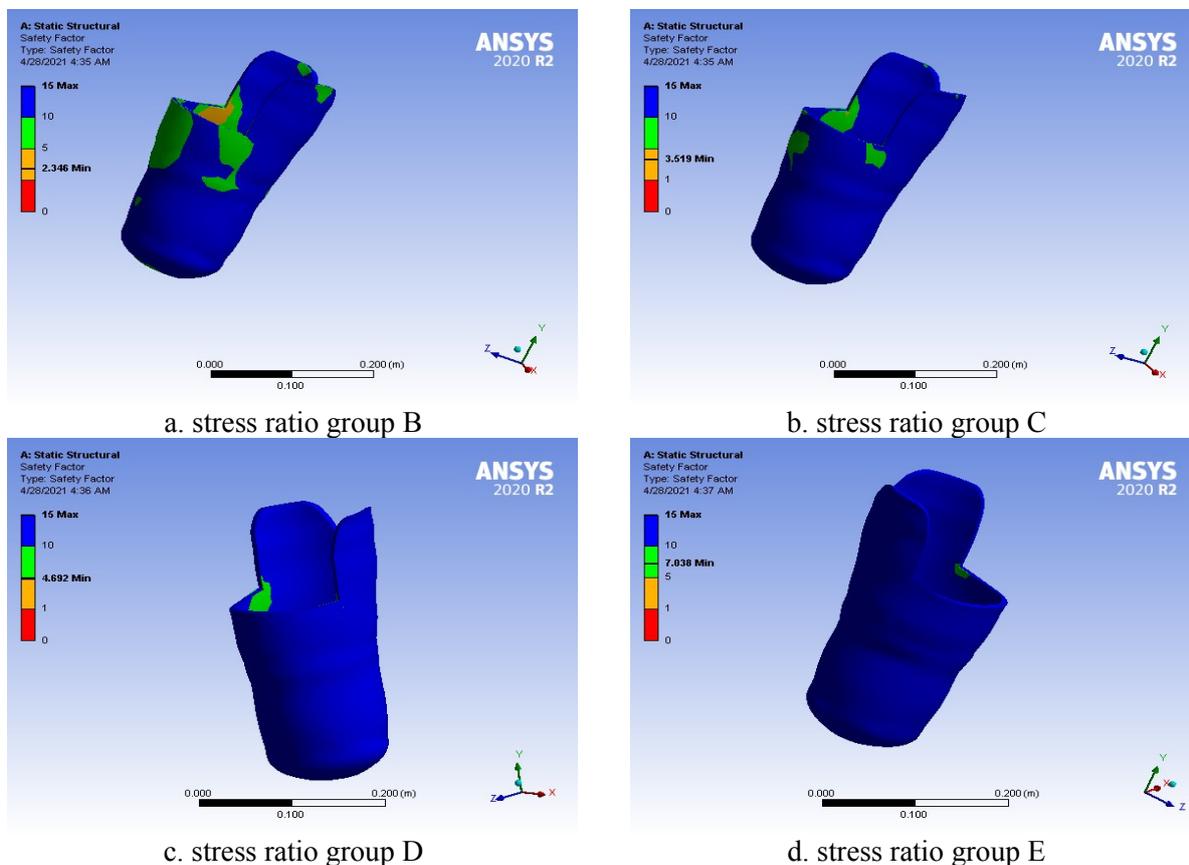


Figure 17. The minimum equivalent safety factor for the lamination without kenaf prosthetic socket (group G) for f-socket with different values of stress ratio.

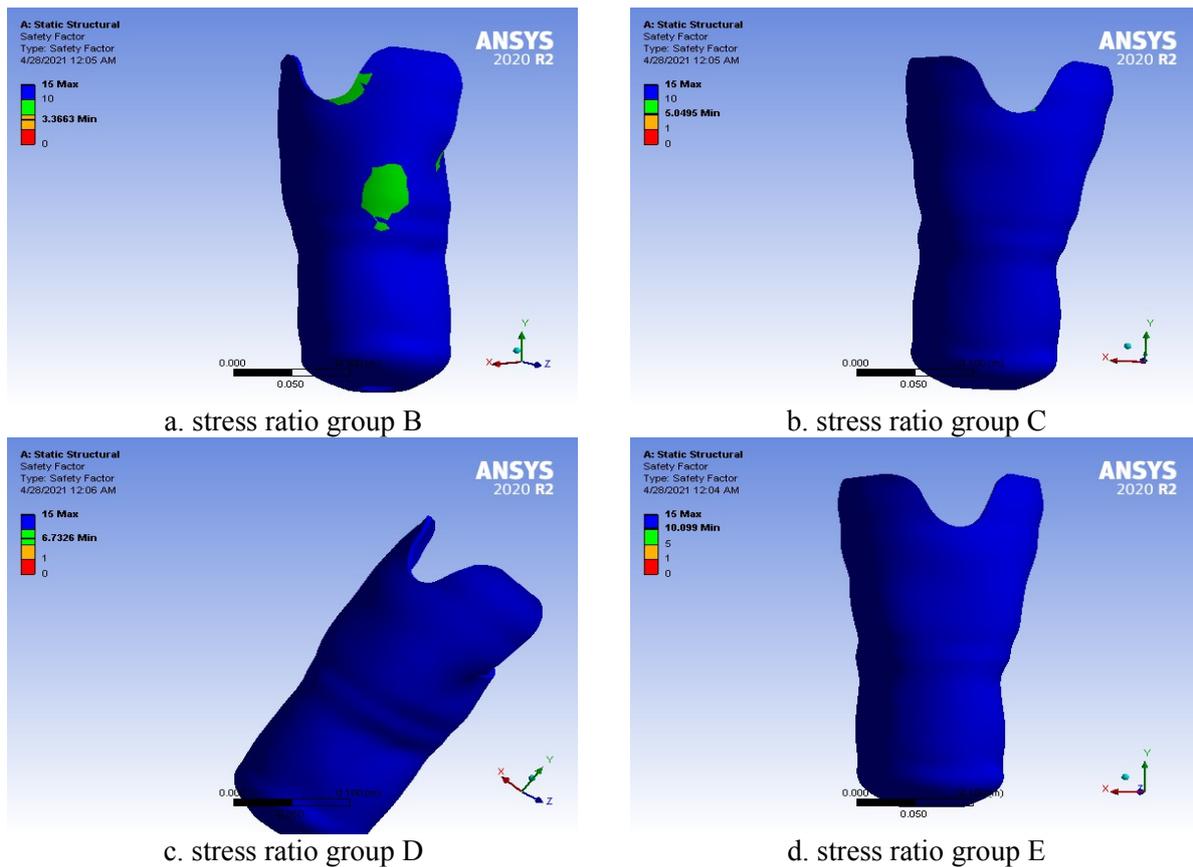


Figure 18. The minimum equivalent safety factor for the lamination with kenaf prosthetic socket (group D) for f-socket with different values of stress ratio.

## 5. Conclusions

From the experimental and numerical investigation for fatigue characterization of composite materials with effect of natural reinforcement fiber, get the following important conclusion as,

1. Group D\_f with kenaf show better results at the mechanical properties than group G, where the strength is increased by (39.35%) and modulus of elasticity (4.23%). The endurance limits were improved by (38.97%) this enhancement has advantages for kenaf lamination materials in manufacturing prostheses can be shown that the modifying for fatigue behavior for composite materials reinforcement with kenaf.
2. Safety factors are higher with kenaf lamination improved 22.3% at 165kpa and 59.49% for f- socket test, it was observed that the arrangement of the layers relative to the proposed material had a positive effect on the safety factor, the deformation of the material and the comfort of the patient during movement.
3. Notice that increasing the stress ratio leads to increasing safety factor at 165 kpa and at f-socket investigation.
4. The 165 kpa the analysis of patient's weight method can be adopted to analyze the socket, but the design will lead to an increase in cost due to the increase in the safety factor.

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